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## LETTER TO THE EDITOR

### Low firing-rates in a compartmental model neuron

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**Abstract.** A nonlinear relationship is obtained between the membrane potential of a compartmental model neuron as a function of input stimulation. This is used to show how shunting effects can lead to low output firing-rates in associative memory networks.

In a recent paper, Abbott [1] has shown how shunting effects can lead to a nonlinear relationship between the input current to a neuron's soma and the incident rates of excitatory inputs synapsing on the neuron's dendritic tree. Such a nonlinearity produces a low output firing-rate in the presence of high levels of excitation, thus providing a solution to the problem of high firing-rates found in network models based on neurons whose input current varies linearly with synaptic inputs. When these latter networks are in a state of self-sustained firing corresponding, say, to a dynamical fixed point of an attractor network [2], the neurons tend to fire at their maximum rate. Cortical neurons, on the other hand, tend to operate well below their maximum rate. Such a problem has received considerable attention within the context of associative memory networks, where the self-sustained firing patterns are interpreted as memory states [3-5].

The analysis of Abbott [1] is based on Rall's cable theory of current flow in a passive dendritic tree [6]. A complementary approach to representing the electrical properties of a neuron's dendritic tree is to use a compartmental model [7]. In this model, the dendritic system is divided into sufficiently small regions or compartments, such that spatial variations of the electrical properties within a region are negligible. The advantage of the compartmental approach, which is used extensively in computational studies of neuronal systems [8], is that it provides a greater flexibility in modelling neurons and a greater economy of computation.

In this letter, we derive an analogous result to Abbott's [1], *vis-à-vis* the effects of shunting on the firing-rate of a neuron, using recent work on temporal pattern processing in a compartmental model neuron [9]. (In [1], a compartmental model neuron is used in computer simulations rather than as the basis of analytical work.) We assume that the compartmental model neuron consists of a soma connected to a single dendritic tree idealized as a one-dimensional chain of  $2M+1$  compartments labelled  $\alpha = -M, \dots, M$ . The equivalent circuit of the  $\alpha$ th compartment consists of a membrane leakage resistor  $R_\alpha$  in parallel with a capacitor  $C_\alpha$ , with the ground representing the extracellular medium (assumed to be an isopotential). Each compartment is joined to its immediate neighbours in the chain by the junctional resistors  $R_{\alpha\alpha-1}$  and  $R_{\alpha\alpha+1}$ . Assuming that each compartment  $\alpha$  has  $N$  synapses labelled  $(\alpha k)$ ,  $k = 1, \dots, N$ , then the current at synapse  $(\alpha k)$  is governed by a time-varying conductance  $\Delta g_{\alpha k}$  in series

with a fixed reversal potential  $S_{\alpha k}$ . It then follows from Kirchoff's law that the time evolution of the membrane potentials  $V_\alpha$  is given by

$$C_\alpha \frac{dV_\alpha}{dt} = -\frac{V_\alpha}{R_\alpha} + \sum_{\langle \beta; \alpha \rangle} \frac{V_\beta - V_\alpha}{R_{\alpha\beta}} + \sum_{k=1}^N \Delta g_{\alpha k} [S_{\alpha k} - V_\alpha] \quad (1)$$

where  $\langle \beta; \alpha \rangle$  indicates that the summation over  $\beta$  is restricted to immediate neighbours of  $\alpha$ . The last term on the right-hand side of equation (1) incorporates shunting effects; the change in a compartment's membrane potential induced by a synaptic input depends on the size of the deviation of the membrane potential from the resting potential. Since each  $\Delta g_{\alpha k}$  is positive, the effect of each term  $\Delta g_{\alpha k} [S_{\alpha k} - V_\alpha]$  is for  $V_\alpha$  to tend towards  $S_{\alpha k}$ . Hence positive and negative  $S_{\alpha k}$  correspond respectively to excitatory and inhibitory synapses.

To obtain a complete picture of the input-output response of a neuron, it is necessary to supplement the leaky-integrator equations (1) with details concerning action potential generation at the axon hillock of the soma [8]. It will be adequate for our purposes simply to view the soma as a point processor that is isopotential with the dendritic compartment nearest to it, taken to be  $\alpha = 0$ . We shall assume that the neuron fires whenever  $V_0(t)$  exceeds a time-dependent threshold  $h$ . The time-dependence of  $h$  represents the effects of *refractory period*. That is, if  $\Delta t$  denotes the time that has elapsed since the neuron last fired then  $h(\Delta t) = \infty$  for  $0 < \Delta t \leq t_R$  and  $h(\Delta t) = h_0 + h_1 \exp(-\Delta t/\tau_a)$  for  $\Delta t > t_R$  (until the neuron fires again). Here  $t_R$  is the absolute refractory period, whereas  $\tau_a$  determines the relative refractory period.

Since equation (1) is formally linear in  $V = (V_\alpha, \alpha = 0, \pm 1, \dots, \pm M)$ , it may be written as a matrix equation of the form [9, 10]

$$\frac{dV}{dt} = H(t)V(t) + U(t) \quad (2)$$

where  $H_{\alpha\beta}(t) = Q_{\alpha\beta} + \bar{Q}_{\alpha\beta}(t)$

$$Q_{\alpha\beta} = -\frac{\delta_{\alpha,\beta}}{\tau_\alpha} + \frac{\delta_{\beta,\alpha+1}}{\tau_{\alpha\alpha+1}}(1 - \delta_{\alpha,M}) + \frac{\delta_{\beta,\alpha-1}}{\tau_{\alpha\alpha-1}}(1 - \delta_{\alpha,-M}) \quad (3a)$$

$$\frac{1}{\tau_\alpha} = \left[ \sum_{\langle \beta'; \alpha \rangle} \frac{1}{\tau_{\alpha\beta'}} + \frac{1}{C_\alpha R_\alpha} \right] \quad \frac{1}{\tau_{\alpha\beta}} = \frac{1}{C_\alpha R_{\alpha\beta}} \quad (3b)$$

$$\bar{Q}_{\alpha\beta}(t) = -\frac{\delta_{\alpha\beta}}{C_\alpha} \sum_k \Delta g_{\alpha k}(t) \quad U_\alpha(t) = \frac{1}{C_\alpha} \sum_k \Delta g_{\alpha k}(t) S_{\alpha k} \quad (4)$$

Formally, equation (2) may be solved as [9, 11]

$$V(t) = \int_0^t dt' T \left[ \exp \left( \int_{t'}^t dt'' H(t'') \right) \right] U(t') + T \left[ \exp \left( \int_0^t dt'' H(t'') \right) \right] V(0) \quad (5)$$

where  $T$  denotes the time-ordered product,  $T[H(t)H(t')] = H(t)H(t')\theta(t-t') + H(t')H(t)\theta(t'-t)$ , which is required since  $H$  is a time-dependent, non-commuting matrix. The term  $T[\exp(\int_{t'}^t dt'' H(t''))]_{\alpha\beta}$  is the Green's function or response function  $\mathcal{G}(\alpha, t; \beta, t')$  of the system.

In general, equation (5) is difficult to analyse due to the dependence of  $H$  on the time-dependent conductances  $\Delta g_{\alpha k}$ . (Note that this is a direct consequence of the inclusion of shunting effects in equation (1). For if the time-dependent part of  $H$  is absent, as occurs when the shunting term  $-V_\alpha \sum_k \Delta g_{\alpha k}$  is dropped from equation (1),

then the Green function  $\mathcal{G}(\alpha, t; \beta, t')$  reduces to the much simpler form  $[e^{(t-t')Q}]_{\alpha\beta}$ . Therefore, we shall make two major simplifying assumptions concerning  $\Delta g_{\alpha k}$  to facilitate our analysis [9]: (i) each action potential and post-synaptic potential is idealized as a Dirac delta-function spike, i.e. details of pulse-shape are neglected and (ii) the arrival times of the action potentials are restricted to be integer multiples of a fundamental unit of time  $t_D$ . The time varying conductance  $\Delta g_{\alpha k}(t)$  induced by an incoming stream of action potentials is then a sequence of conductance spikes of the form

$$\Delta g_{\alpha k}(t) = \varepsilon_{\alpha k} \sum_{m \geq 0} \delta(t - mt_D) a_{\alpha k}(m) \quad (6)$$

where  $a_{\alpha k}(m) = 1$  if an action potential arrives at the discrete time  $mt_D$  and is zero otherwise. The size of each conductance spike,  $\varepsilon_{\alpha k}$ , is determined by factors such as the amount of neurotransmitter released on arrival of an action potential and the efficiency with which these neurotransmitters bind to receptors [11].

The discrete time condition imposed on the arrival times, assumption (ii), means that the inputs to the neuron are specified completely by the sequence of patterns  $A(m) = (a_{\alpha k}(m), \alpha = 0, \pm 1, \dots, \pm M, k = 1, \dots, N)$ , integer  $m$ . Each pattern  $A(m)$  is a  $(2M + 1) \times N$  matrix. We shall use a more concise representation of an input pattern by assuming that each compartment consists of two groups of identical synapses, one excitatory and the other inhibitory. The input  $A(m)$  is then specified by the set  $\{N_{\alpha}^{(e)}(m), N_{\alpha}^{(i)}(m)\}$  where  $N_{\alpha}^{(e)}(m), N_{\alpha}^{(i)}(m)$  are the number of excitatory and inhibitory synapses respectively that receive an action potential at time  $m$ . Substituting equation (6) into (4) and using this representation of input patterns we obtain

$$\begin{aligned} \bar{Q}_{\alpha\beta}(t) &= \delta_{\alpha\beta} \sum_{m \geq 0} \delta(t - mt_D) q_{\alpha}(m) & U_{\alpha}(t) &= \sum_{m \geq 0} \delta(t - mt_D) u_{\alpha}(m) & (7) \\ q_{\alpha}(m) &= \varepsilon_{\alpha}^{(e)} N_{\alpha}^{(e)}(m) + \varepsilon_{\alpha}^{(i)} N_{\alpha}^{(i)}(m) & & & (8) \\ u_{\alpha}(m) &= \varepsilon_{\alpha}^{(e)} S^{(e)} N_{\alpha}^{(e)}(m) + \varepsilon_{\alpha}^{(i)} S^{(i)} N_{\alpha}^{(i)}(m) \end{aligned}$$

where for convenience the capacitance  $C_{\alpha}$  has been absorbed into each  $\varepsilon_{\alpha}^{(e,i)}$  so that  $\varepsilon_{\alpha}^{(e,i)}$  is dimensionless. The excitatory and inhibitory reversal potentials  $S^{(e,i)}$  are taken to be  $\alpha$ -independent. Observe that  $S^{(e)}, \varepsilon_{\alpha}^{(e,i)} > 0$  whereas  $S^{(i)} \leq 0$ .

The presence of Dirac delta-functions in equation (7) allows the integrals in (5) to be performed explicitly. In particular, the time-ordered product may be calculated using standard path-integral techniques to give, on setting  $t_D = 1$  and  $V(0) = 0$  [9]

$$V_{\alpha}(t) = \sum_{\beta} [e^{(t-m)Q} e^{-G(m)}]_{\alpha\beta} X_{\beta}(m) \quad m < t < m + 1 \quad (9)$$

for all positive integers  $m$ , where  $G_{\alpha\beta}(m) = \delta_{\alpha\beta} q_{\alpha}(m)$  and  $u_{\alpha}(m), q_{\alpha}(m)$  satisfy equation (8). Here  $X_{\beta}$  is a discrete-time variable defined iteratively according to  $X_{\alpha}(0) = u_{\alpha}(0)$  and, for  $m > 0$

$$X_{\alpha}(m) = \sum [e^Q e^{-G(m-1)}]_{\alpha\beta} X_{\beta}(m-1) + u_{\alpha}(m). \quad (10)$$

The main effect of shunting is to alter the local decay-rate of a compartment according to  $1/\tau_{\alpha} \rightarrow 1/\tau_{\alpha} + q_{\alpha}(m)/(t-m)$  for  $m < t \leq m + 1$ . Since each  $q_{\alpha}$  is proportional to the number of concurrent inputs to the  $\alpha$ th compartment (equation (8)), this suggests a mechanism whereby shunting can limit the size of response of the neuron. That is, constant high rates of stimulation can lead to fast rates of decay so that the steady-state values of the membrane potentials are lower than those that would occur

in the absence of shunting. To show how this can occur, we shall determine the steady-state values of the variables  $X_\alpha(m)$  in the presence of constant synaptic inputs. Suppose that the  $L$ th compartment receives excitatory inputs at a constant rate  $E$  whilst every other compartment receives inhibitory inputs at a constant rate  $F$ . In other words,  $N_\alpha^{(e)}(m) = E\delta_{\alpha L}$ ,  $N_\alpha^{(i)}(m) = F(1 - \delta_{\alpha L})$  for all  $m$ . Furthermore we shall take  $\varepsilon_\alpha^{(e,i)}$  to be  $\alpha$ -independent with  $\varepsilon^{(i)}F = \varepsilon^{(e)}E$ , and set  $S^{(i)} = 0$ . (An analogous pattern of stimulation is considered by Abbott [1].) Then using equations (8) and (10) we obtain

$$X_\alpha(m) = \varepsilon^{(e)}S^{(e)}E \sum_{n=0}^m [\exp(nQ(E))]_{\alpha L} \quad (11)$$

where  $Q(E)_{\alpha\beta} = Q_{\alpha\beta} + \delta_{\alpha\beta}\varepsilon^{(e)}E$ .

It remains to determine the matrix  $\exp(Q(E))$ . As shown in [9], many of the qualitative features of the model can be determined by assuming that all compartments have identical properties and taking the limit  $M \rightarrow \infty$ . (In the case of an infinite dendritic chain, we do not have to worry about edge effects arising from the compartments at  $\pm M$ .) Setting  $R_\alpha = R$ ,  $C_\alpha = C$ ,  $R_{\alpha\alpha+1} = \bar{R}$  for all  $\alpha$  in equation (3) gives  $\tau_\alpha = \tau$ ,  $\tau_{\alpha\alpha+1} = \gamma = \tau_{\alpha+1\alpha}$  where  $1/\tau = 2/\gamma + 1/\bar{\tau}$ ,  $\gamma = \bar{R}C$ ,  $\bar{\tau} = RC$ . Using standard results from the theory of random walks, it follows that for a uniform, infinite dendritic chain [9],  $[\exp(nQ(E))]_{\alpha\beta} = \exp(-n/\tau - n\varepsilon^{(e)}E) I_{|\alpha-\beta|}(2n/\gamma)$  where  $I_n$  is the modified Bessel function of integer order. The steady-state value of  $X_\alpha(m)$  is then given by

$$X_\alpha^\infty = \varepsilon^{(e)}S^{(e)}E \lim_{m \rightarrow \infty} \sum_{n=0}^m \exp\left(-n\left(\frac{1}{\tau} + \varepsilon^{(e)}E\right)\right) I_{|L-\alpha|}(2n/\gamma). \quad (12)$$

The series on the right-hand side of (12) is convergent so that the steady-state  $X^\infty$  is well-defined. Note that  $X^\infty$  determines the long-term behaviour of the membrane potentials  $V$  according to equation (9); we shall refer to  $X_\alpha^\infty$  as the *steady-state membrane potential* of the  $\alpha$ th compartment. For small levels of excitation  $E$ ,  $X_\alpha^\infty$  is approximately a linear function of  $E$ . However, as  $E$  increases, the contribution of shunting inhibition to the effective decay-rate becomes more and more significant so that  $X_\alpha^\infty$  eventually begins to decrease. This is illustrated in figure 1, where  $X_0^\infty/S^{(e)}$  is plotted as a function of  $\varepsilon^{(e)}E$  for  $\bar{\tau} \gg \gamma$ ,  $\gamma = 1$  and  $L = 1$  in equation (12) (cf figure 3 of [1]).

Finally, using similar arguments to Abbott [1] it can be shown that the nonlinear relationship between  $X_\alpha^\infty$  and  $E$  in equation (12) provides a solution to the problem of high firing-rates. First, it is necessary to determine the output firing-rate of the

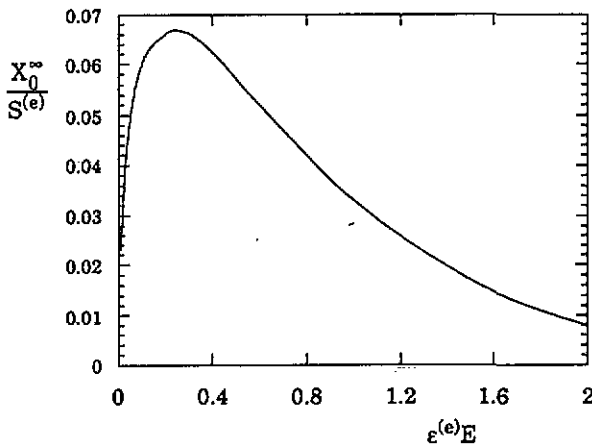


Figure 1. Steady-state value of the membrane potential at the soma as a function of the excitatory rate of inputs to the compartment at  $\alpha = 1$ .

neuron. In the presence of constant inputs, the membrane potential at the soma will reach some (time-averaged) steady-state  $\bar{V}_0$ . The larger  $\bar{V}_0$ , the faster the decreasing threshold  $h(\Delta t)$  is crossed from below after firing and thus the greater the firing-rate  $z$  of the neuron. As shown by Amari [12], a reasonable approximation for  $z$  is a sigmoid function of  $\bar{V}_0$ . Hence, noting from (9) and (12) that  $\bar{V}_0 \propto X_0^\infty$ , the average firing-rate of the neuron is  $z = f(E) = f_{\max} / (1 + \exp[g(\kappa - X_0^\infty(E))])$  for some gain  $g$  and threshold  $\kappa$ . Here  $f_{\max}$  is the maximum firing-rate, which is determined by the absolute refractory period.

Now consider a population of excitatory neurons in which the effective excitatory rate  $E$  impinging on a neuron is determined by the average firing-rate ( $z$ ) of the population. Similarly, the inhibitory rate  $F$  is determined by the average firing-rate of a population of inhibitory interneurons. For a self-consistent picture, it is necessary to restrict the firing times of the neurons to be integer multiples of  $t_D$ . However, since  $t_D$  could be made arbitrarily small, this is not a serious restriction. Alternatively, we can simply interpret equation (10) as representing a discrete time, compartmental model neuron with the  $X_\alpha$  identified as the state variables of the neuron and, say,  $f/f_{\max}$  equal to the probability that the neuron fires at each time step. (Such a discrete time model is a natural extension of the standard binary neuron used in artificial neural networks that incorporates spatio-temporal aspects of real neurons.) For a large population of neurons, a reasonable approximation is to take  $E = c\langle z \rangle$ , for some constant  $c$ . Within a mean-field approach, the steady-state behaviour of the population is then determined by the self-consistency condition  $E = cf(E)$  [1]. Using graphical methods one finds that there are two stable solutions to this equation, one corresponding to the silent state  $E = 0$  and the other to a state in which the firing-rate is considerably below  $f_{\max}$ . On the other hand, if  $X_0^\infty$  were a linear function of  $E$  then this latter stable state would have a firing-rate close to  $f_{\max}$ .

This is illustrated by curve (b) of figure 2 where  $f/f_{\max}$  is plotted as a function of  $E$  with  $X_0^\infty$  satisfying (12),  $\varepsilon^{(e)}cf_{\max} = 1$ , and  $g^{-1} = 0.03$ ,  $\kappa = 1.0$ . On the other hand, if  $X_0^\infty$  is a linear function of  $E$ , i.e., the contribution of the term  $\varepsilon^{(e)}E$  to the exponential in equation (12) is dropped, then this latter stable state has a firing-rate close to  $f_{\max}$ , see curve (a) of figure 2. (The proof of these results is identical to that of [1].) Note that for certain choices of parameter values there is an additional solution to the self-consistency condition but this is unstable.

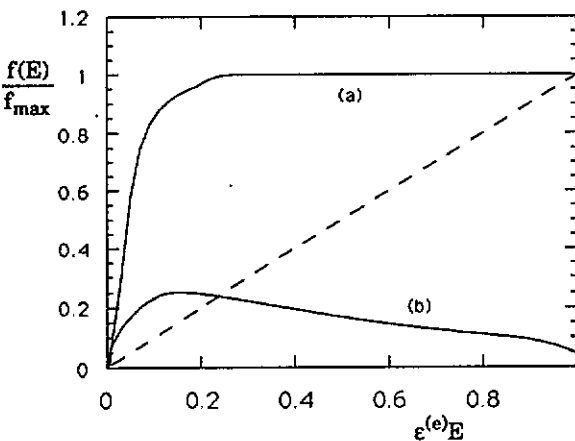


Figure 2. Firing-rate/maximum firing-rate  $f/f_{\max}$  as a function of input excitation  $E$  for (a) linear and (b) nonlinear relationship between steady-state membrane potential  $X_0^\infty$  and  $E$ . Points of intersection with straight line are states of self-sustained firing.

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